



New Filters for Image Interpolation and Resizing

Amir Said
Media Technologies Laboratory
HP Laboratories Palo Alto
HPL-2007-179
November 2, 2007*

interpolation kernels,
image processing,
image resizing

We propose a new set of kernels to simplify the design of filters for image interpolation and resizing. Their properties are defined according to two parameters, specifying the width of the transition band and the height of a unique sidelobe. By varying these parameters it is possible to efficiently explore the space with only the filters that are suited for image interpolation and resizing, and identify the filter that is best for a given application. These two parameters are also sufficient to obtain very good approximations of many commonly-used interpolation kernels. We also show that, because the Fourier transforms of these kernels have very fast decay, these filters produce better results when time-stretched for image downsizing.

* Internal Accession Date Only

Approved for External Publication

This report contains material published in the 2007 IEEE International Conference on Image Processing, Copyright
© IEEE 2007

New Filters for Image Interpolation and Resizing

Amir Said

Hewlett Packard Laboratories, Palo Alto, CA

Abstract

We propose a new set of kernels to simplify the design of filters for image interpolation and resizing. Their properties are defined according to two parameters, specifying the width of the transition band and the height of a unique sidelobe. By varying these parameters it is possible to efficiently explore the space with only the filters that are suited for image interpolation and resizing, and identify the filter that is best for a given application. These two parameters are also sufficient to obtain very good approximations of many commonly-used interpolation kernels. We also show that, because the Fourier transforms of these kernels have very fast decay, these filters produce better results when time-stretched for image downsizing.

1 Introduction

Image resizing and interpolation (e.g., for rotation) are two of the most useful image processing operations, and consequently there is a great amount of literature on the subject [1]–[8]. However, many imaging professionals find the task of sorting out and implementing the most appropriate method quite challenging, due to the great number of possibilities, and of conflicting opinions. It is common to settle for some very simple approaches which were once meant to reduce complexity, or adopt one type that was shown to be excellent for one application, without knowing that it may be suboptimal for other applications.

For instance, even in commercial products we find the mistake of using interpolation kernels for downsampling without the necessary lowpass filtering. A less serious, but also common mistake, is to use for downsampling low-order filters which can be quite good for interpolation, but have much worse properties when time-scaled for downsizing.

What is still missing is an approach that is more *convenient and easy to use*, with less emphasis on computational complexity, and that yields high image quality. For that purpose we propose a family of parameterized functions that are simple, and are designed with enough

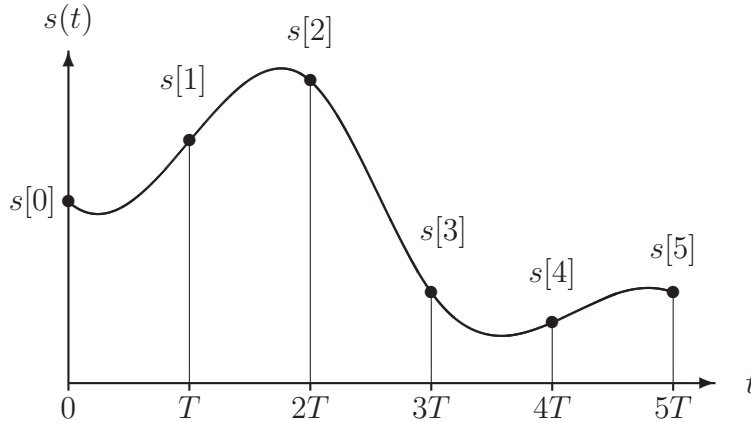


Figure 1: A signal $s(t)$ that is sampled with period T .

versatility so that well-known kernels can be very closely approximated by simply using the proper parameters. This way it is easy to experiment and identify the parameters that are best suited to a certain type of image, without having to understand and implement several methods.

This paper is organized by first having a very brief review of sampling and interpolation concepts, which allow us to establish the notation. Next we define the proposed family of functions, and some of their basic properties. We present a set of features that are desirable for interpolation and resizing kernels, and explain how well the proposed functions support those features. Finally, we present some results of finding the approximation to some commonly-used kernels, show how well these kernels are approximated, and discuss some features of the proposed kernels.

2 Signal Sampling and Reconstruction

Even though this work is about two-dimensional images, to simplify the notation we assume that only separable filters are used [4], and thus consider only the one-dimensional cases. In practice separable filters are almost always used because of their much lower computational complexity.

In our analysis of sampling and reconstructing signals, we consider a function $s(t)$ with Fourier transform

$$S(f) = \int_{-\infty}^{\infty} s(t) e^{-j2\pi ft} dt, \quad (1)$$

that is sampled with period T , as shown in Figure 1, to generate the sequence

$$s[n] = s(nT), \quad n \in \mathbb{Z}. \quad (2)$$

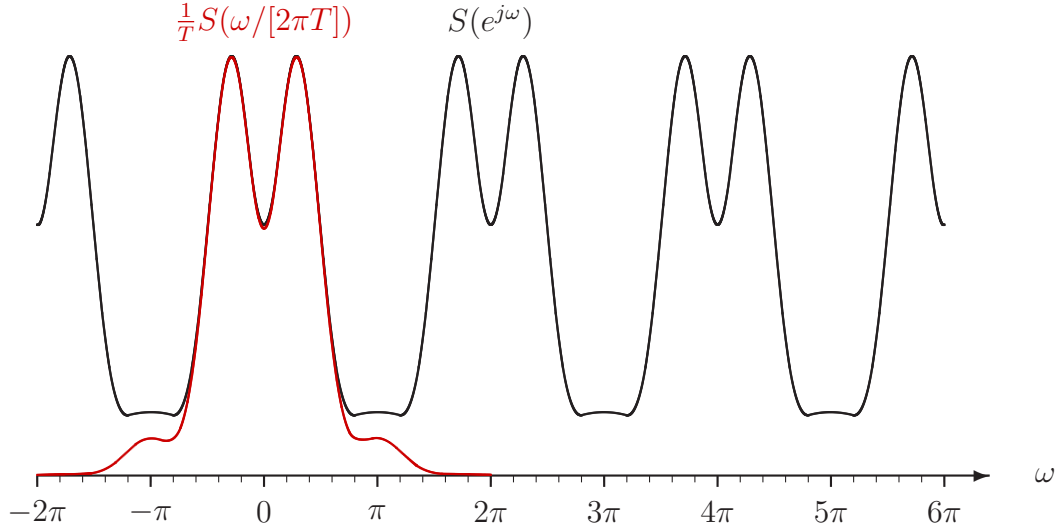


Figure 2: A signal spectrum and the Fourier Transform of its sampled sequence.

The Fourier transform of this sequence is

$$S(e^{j\omega}) = \sum_{n=-\infty}^{\infty} s[n] e^{-j\omega n}. \quad (3)$$

Note that we use the notation of reference [3], using parenthesis for functions of real variables and brackets for functions of integer variables.

From the sampling theorem [3, 4] we have, for $\omega = 2\pi fT$,

$$S(e^{j\omega}) = \frac{1}{T} \sum_{n=-\infty}^{\infty} S\left(\frac{\omega}{2\pi T} - \frac{n}{T}\right), \quad (4)$$

or, equivalently,

$$S(e^{j2\pi fT}) = \frac{1}{T} \sum_{n=-\infty}^{\infty} S\left(f - \frac{n}{T}\right). \quad (5)$$

Figure 2 shows in red an example of the bandlimited spectrum of a signal $s(t)$, and the corresponding periodic spectrum of its sampled sequence. We can note that in this example the bandwidth of the signal is larger than $1/(2T)$, so there is overlap in the shifted versions of $S(f)$, i.e., *aliasing* [3].

Given a reconstruction kernel $\phi(t)$, with Fourier transform $\Phi(f)$, we define a *reconstructed*

function

$$r(t) = \sum_{k=-\infty}^{\infty} s[k] \phi\left(\frac{t}{T} - k\right), \quad (6)$$

which has Fourier transform

$$R(f) = T S(e^{j2\pi fT}) \Phi(fT) \quad (7)$$

$$= \Phi(fT) \sum_{k=-\infty}^{\infty} S\left(f - \frac{k}{T}\right). \quad (8)$$

From this equation we can observe that if the signal $s(t)$ is strictly bandlimited, i.e., if its spectrum satisfies

$$S(f) = 0, \quad \forall f \notin \left(-\frac{1}{2T}, \frac{1}{2T}\right) \quad (9)$$

then we can have $R(f) = S(f)$, and consequently $r(t) = s(t)$, if we use as $\phi(t)$ the box (ideal filter) kernel

$$b(t) = \frac{\sin(\pi t)}{\pi t}, \quad (10)$$

which has Fourier transform

$$B(f) = \begin{cases} 1, & |f| < 1/2, \\ 1/2, & |f| = 1/2, \\ 0, & |f| > 1/2, \end{cases} \quad (11)$$

If we resample $r(t)$ with period τ , we have

$$r[n] = r(n\tau) = \sum_{k=-\infty}^{\infty} s[k] \phi\left(\frac{n\tau}{T} - k\right) \quad (12)$$

and defining

$$\gamma = \frac{T}{\tau}, \quad (13)$$

we obtain

$$R(e^{j2\pi f}) = \gamma \sum_{n=-\infty}^{\infty} \Phi(\gamma[f - n]) S(e^{j2\pi\gamma[f-n]}). \quad (14)$$

From this result it is clear that we can only have $R(e^{j\omega}) = S(e^{j\omega})$ when $T = \tau$ and $\phi(t) = b(t)$. However, if $\tau \leq T$ and $s(t)$ satisfies (9), then we can preserve all information on $s(t)$ using $\phi(t) = b(t)$. If, on the other hand, we have $\tau > T$, then spectrum of $R(f)$ has to satisfy

$$R(f) = 0, \quad \forall f \notin \left(-\frac{1}{2\tau}, \frac{1}{2\tau}\right) \quad (15)$$

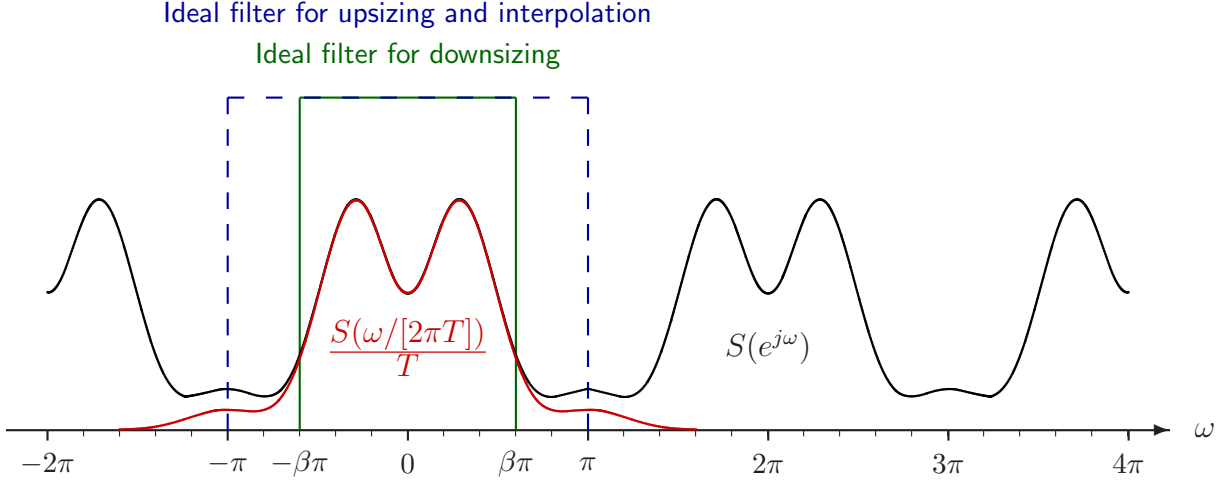


Figure 3: Box filters used for strictly bandlimited signals.

to avoid aliasing. This can be done by using a time-stretched version $\phi(t) = \gamma b(\gamma t)$ as the reconstruction kernel.

Figure 3 shows the two cases, when ideal (box) filters are used. When $\tau \leq T$ (upsampling and interpolation) the filter response covers the whole original bandwidth, and when $\tau > T$ (downsampling) the filter response is reduced by a factor T/τ to avoid aliasing.

In conclusion, when it is known that a signal that has been sampled with period T needs to be resampled with period τ , we can use the kernels

$$\phi(t) = \beta b(\beta t), \quad (16)$$

where

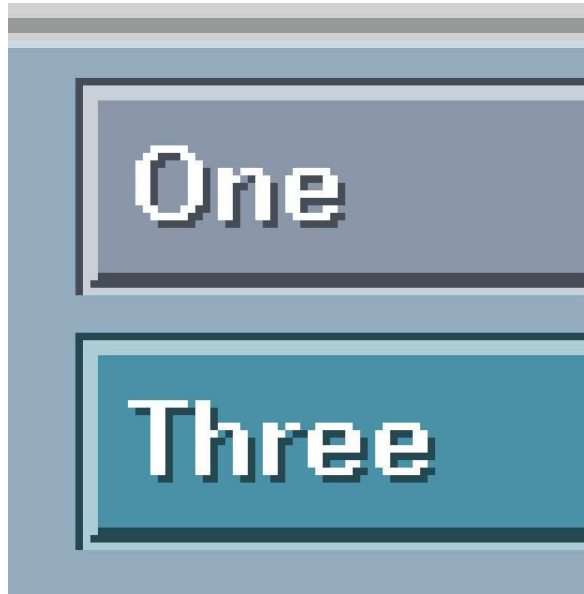
$$\beta = \min(1, T/\tau). \quad (17)$$

3 Kernels for Image Interpolation and Resizing

The theory presented in Section 2 was developed for analyzing exact recovery of sampled signals that are strictly bandlimited. In image applications we normally do not have signals that are truly bandlimited. One common example is in the images containing text, which define discontinuous signals. The application of ideal filters to those images produces highly visible “ringing” artifacts, as shown in Figure 4(a). Thus, other types of filters had been used



(a)



(b)



(c)



(d)

Figure 4: Examples of an image with text interpolated using different kernels. (a) Ideal bandlimited filter; (b) Pixel replication kernel; (c) “Screen door” effect caused by insufficient attenuation of repeated versions of the spectrum; (d) cubic spline kernel.

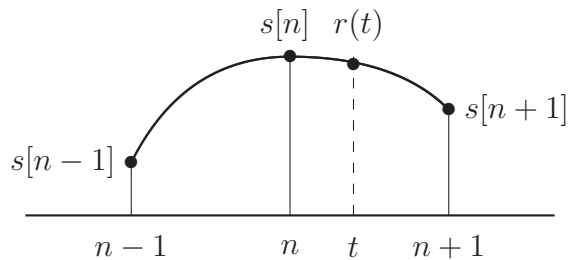


Figure 5: Notation used for interpolation and resizing.

for images [1]–[8]. For upsizing by integer factors, the simplest technique is to just replicate the pixel values, but as can be seen in Figure 4(b), the results are also visually quite bad.

Another problem occurs when the filters do not remove enough of the periodic versions in the spectrum of the sampled signal. In this case we have the “screen door” effect, as shown in Figure 4(c). Much better results are obtained using some kernels defined for general function interpolation. For instance, Figure 4(d) shows the image obtained with cubic-spline interpolation.

Figure 5 shows the basic notation we use. We assume $T = 1$, and for a sequence of signal values $s[n]$, and an interpolation kernel function $h(t)$,¹ the reconstructed value at point t is defined as

$$r(t) = \beta \sum_{i=-\infty}^{\infty} s[i]h(\beta[t - i]). \quad (18)$$

where β is the normalized bandwidth of the signal, as defined by (17). When downsampling the image factor β should be equal or smaller than the reduction factor, which means that $0 < \beta < 1$. When the image is upsampled or rotated, we have $\beta = 1$.

This series can be also defined as

$$r(t) = \beta \sum_{k \in S_h} s[k + \lfloor t \rfloor]h(\beta[t - k - \lfloor t \rfloor]), \quad (19)$$

where S_h is a range of integers defined by the condition $h(\beta t) \neq 0$. In practice, we can use the condition $|h(\beta t)| < \epsilon$, where ϵ is sufficiently small.

Using the new notation with interpolation kernels, if we resample $r(t)$ with period τ , we have the convolution

$$r[n] = r(n\tau) = \beta \sum_{k=-\infty}^{\infty} s[\eta_n - k]h_{\alpha_n, \beta}[k], \quad (20)$$

¹In Section 2 we use $\phi(t)$ in the analysis of strictly bandlimited signals. In the rest of this document we use $h(t)$ to identify the type of kernels that are used in practice.



Figure 6: Arrays with sequence of filter coefficients that are pre-computed for image resizing, and repeatedly used in the vertical (or horizontal) resampling computations.

where

$$\eta_n = \lfloor n\tau \rfloor, \quad (21)$$

$$\alpha_n = n\tau - \lfloor n\tau \rfloor, \quad (22)$$

$$h_{\alpha, \beta}[k] = h(\beta[k + \alpha]). \quad (23)$$

This means that the new sequence has each sample defined by a convolution sum, but the coefficients can be different in each case. When the ratio T/τ is integer or rational, the sets of coefficients occur periodically, and we have a multi-rate system.

For image applications it is commonly more efficient to pre-compute and store sequentially all the coefficients of these convolutions in a single array (cf. Figure 6), which are later repeatedly used when the images lines are resampled. Only one set is needed for the vertical resizing, and another for the horizontal resizing.

4 New Kernel for Interpolation and Resizing

The family of functions that we propose for interpolation and resizing has only two parameters, χ and η , and is defined by

$$h_{\chi, \eta}(t) = \text{sinc}(t) \cosh\left(\frac{\sqrt{2\eta}\pi\chi t}{2 - \eta}\right) e^{-[\pi\chi t/(2-\eta)]^2} \quad (24)$$

where

$$\text{sinc}(t) = \begin{cases} 1, & t = 0, \\ \sin(\pi t)/(\pi t), & t \neq 0, \end{cases} \quad (25)$$

The Fourier transforms of these functions are

$$H_{\chi, \eta}(f) = P_\eta\left(\frac{[2f + 1][2 - \eta]}{\sqrt{2}\chi}\right) - P_\eta\left(\frac{[2f - 1][2 - \eta]}{\sqrt{2}\chi}\right) \quad (26)$$

where

$$P_\eta(f) = \frac{e^{\eta/2}}{\sqrt{2\pi}} \int_0^f e^{-\phi^2/2} \cos(\sqrt{\eta}\phi) d\phi \quad (27)$$

Figures 7, 8, and 9 show some examples. Note that all graphs have $|h_{\chi,\eta}(t)|$ and $|H_{\chi,\eta}(f)|$ in decibels. We can observe that χ basically controls the width of the transition band, and η affects the height of the first sidelobe. Thus, when $\chi \rightarrow 0$ the functions $H_{\chi,\eta}(f)$ converge to the ideal lowpass filter and

$$H_{0,\eta}(f) = \begin{cases} 1, & |f| < 1/2, \\ 1/2, & |f| = 1/2, \\ 0, & |f| > 1/2. \end{cases} \quad (28)$$

While there is no closed-form expression for integral (27) (related to the complex-valued error function), we used the time-frequency properties of the functions, and found that it can be approximated with absolute error smaller than 10^{-16} using

$$P_\eta(f) \approx \begin{cases} 1/2, & f > 8, \\ \frac{f}{17} + \sum_{n=1}^{22} \frac{e^{-\omega^2 n^2}}{\pi n} \cosh(2\omega n \sqrt{\eta}) \sin(2\omega n f), & |f| \leq 8, \\ -1/2, & f < -8, \end{cases} \quad (29)$$

where $\omega = \pi/17$.

5 Desirable Features

There are some important features—not all simultaneously achievable—that are desirable for the kernel functions used for creating the discrete-time filters.

5.1 Flexibility

It is necessary to recognize that different types of images (natural, medical, synthetic, etc.) have different requirements. While we have a variety of theoretical tools developed for the analysis and design of interpolation and resizing filters, in most cases it is still essential to experiment several filters, and visually inspect the results.

The proposed kernels are meant to allow imaging professionals to try different filters more easily. In fact, to make their performance and visual quality easier to predict, they can closely approximate other commonly used kernels. This way, it is possible to start with those approximations, and see how the image quality is altered after changes in the parameters.

Table 1 shows some sets of parameters that can be used for these approximations, and Figures 12 and 13 show how good the approximation are. (More details in Section 6.)

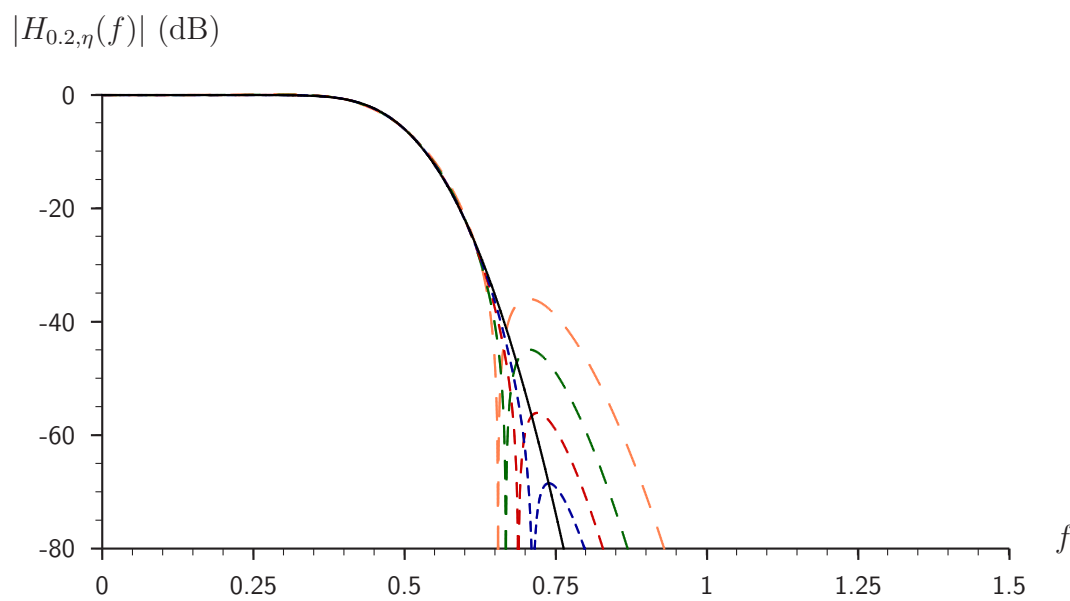
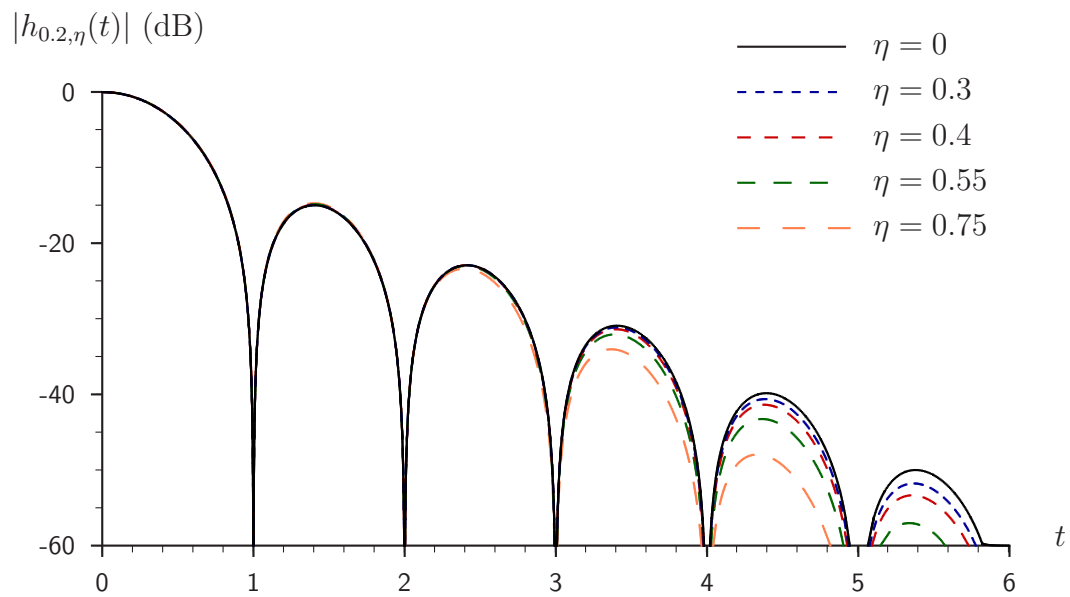


Figure 7: Impulse and frequency responses for some selected parameters, $\chi = 0.2$.

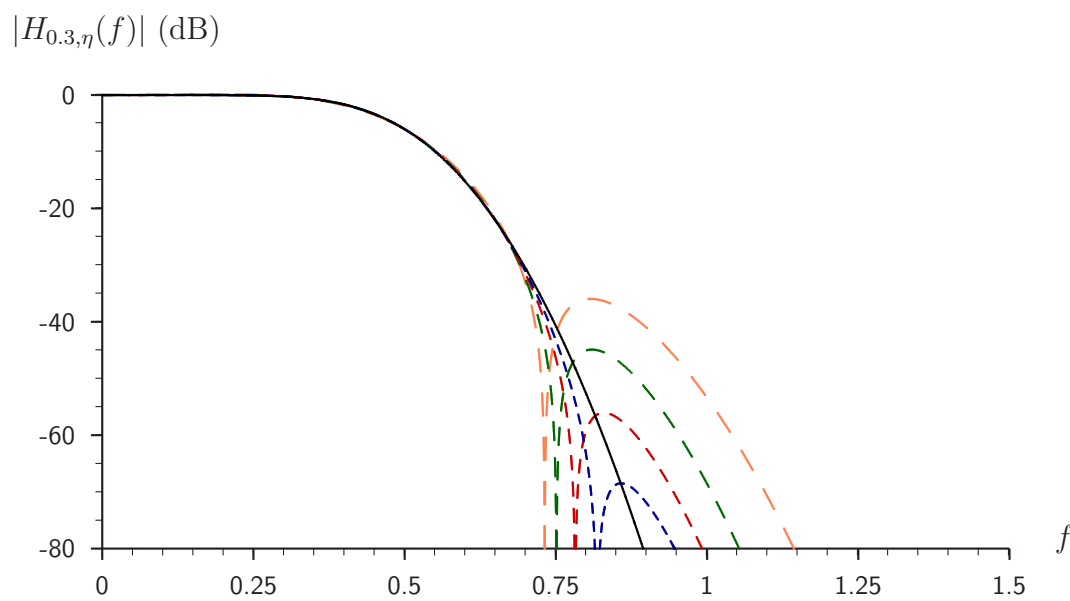
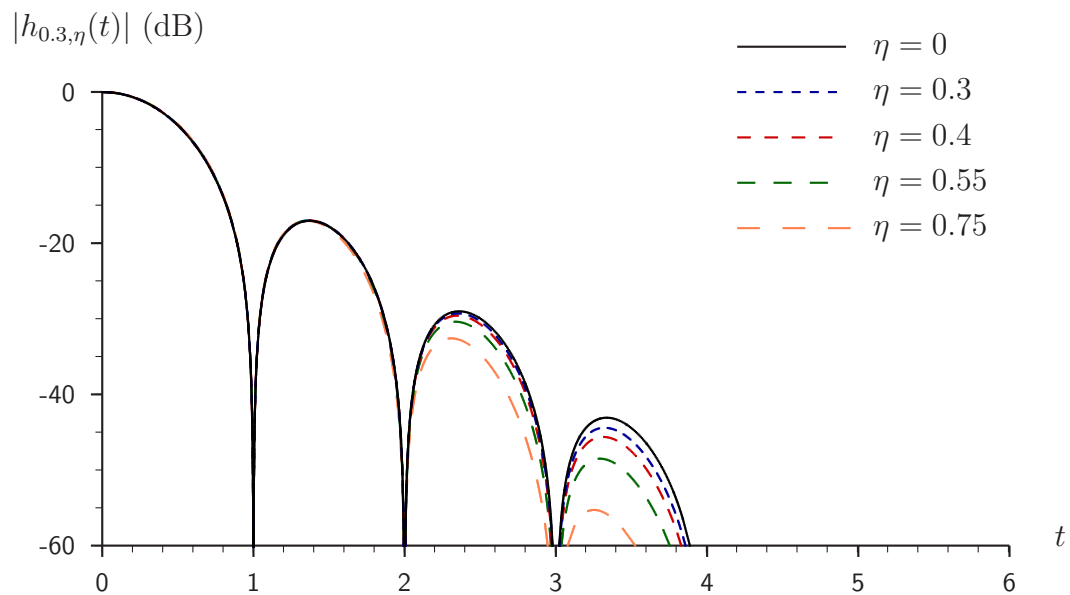


Figure 8: Impulse and frequency responses for some selected parameters, $\chi = 0.3$.

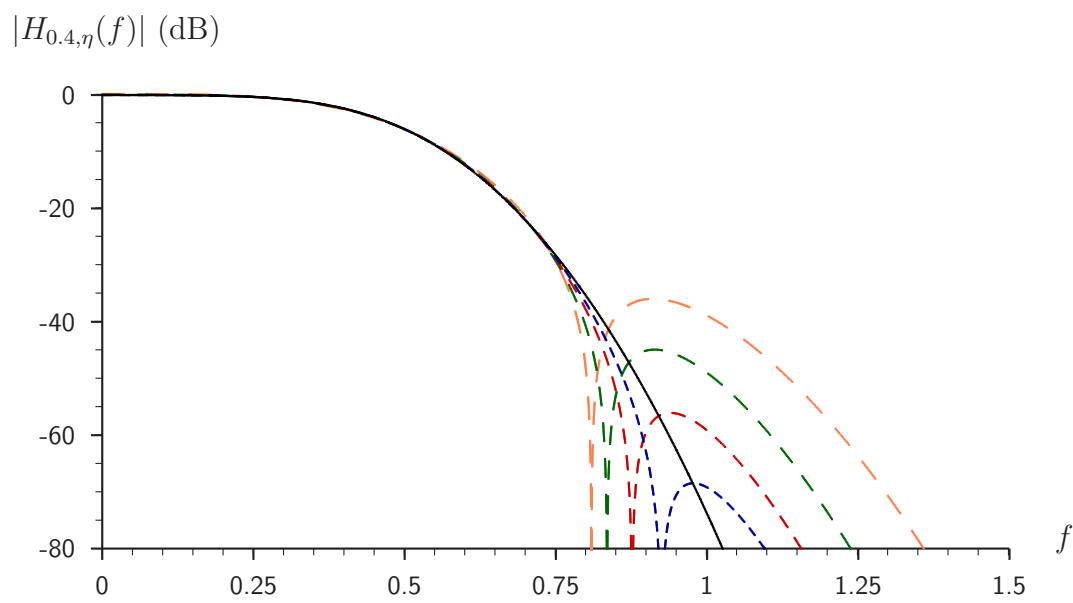
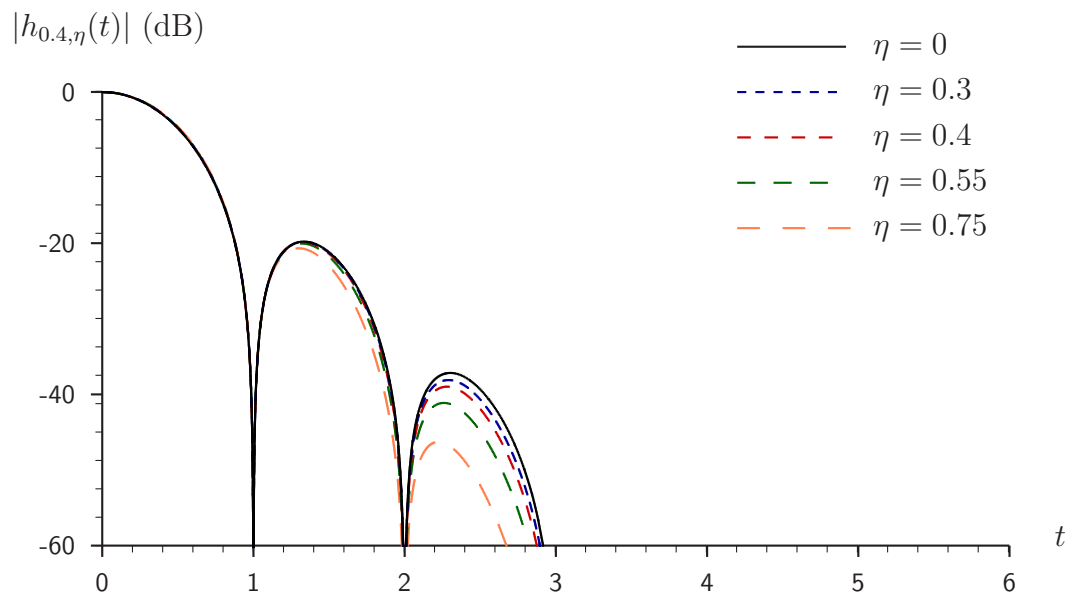


Figure 9: Impulse and frequency responses for some selected parameters, $\chi = 0.4$.

5.2 Intuitive Controls

While experimenting, it is desirable to be able to finely tune the filter’s response. Some kernels provide very little control, being defined only for some discrete parameters, like “order.” Others are defined by parameters related to approximation theory, which may have limited relation to the properties of natural images.

We defined the parameters of our kernel in a way that makes its equations somewhat more complicated, but aiming to make them much more intuitive. The parameter χ is defined to be the main control for achieving a compromise between blurring, aliasing and ringing artifacts. If it is too small, we have nearly ideal filters, which create ringing artifacts around edges. If it is too large we have blurring and the screen door effect. The amount of aliasing depends also on the parameter η , which controls the height of the sidelobe. These properties can be seen in Figures 7 to 9.

5.3 Symmetry and Exact Interpolation

For imaging applications it is necessary to use linear phase filters, and commonly interpolation functions have even symmetry, i.e., $h(t) = h(-t)$. Under the assumption that pixel values corresponds to samples of a strictly bandlimited signal, we would like to not change the values that are already know, and this is achieved when

$$h(0) = 1, \quad h(n) = 0, \quad n = \pm 1, \pm 2, \dots \quad (30)$$

Image signals are certainly not strictly bandlimited, but the property is still useful because it implies that for all f we have

$$H_d(e^{j2\pi f}) = \sum_{n=-\infty}^{\infty} H(f - n) = 1, \quad (31)$$

i.e., we know that the gain for signal plus aliasing always adds to one. Our kernels satisfy this property because they belong to the class of functions created by multiplying $\text{sinc}(t)$ with another function.

5.4 Good Response with Small Spatial Support

When considering the filtering computational complexity, it is good to use filters with small numbers of taps. Since in imaging applications we need to avoid ringing resulting from lowpass filters with steep transition, good interpolation results had been obtained with very short filters.

Our kernels were chosen such that $h_{\chi,\eta}(t)$ and $H_{\chi,\eta}(f)$ have very fast asymptotic decay. In fact, there are constants a, b, c , and d such that

$$\begin{aligned} |h_{\chi,\eta}(t)| &\leq a e^{-bt^2} \\ |H_{\chi,\eta}(f)| &\leq c e^{-df^2}. \end{aligned}$$

Thus, while $h_{\chi,\eta}(t)$ strictly has infinite support, the very fast decay makes it easy to find where to truncate the response without significantly changing the filter's performance (cf. Figures 7 to 9). This approach tends to yield somewhat longer filter responses, but it is more convenient for obtaining downsampling filters, which need to be more carefully designed.

5.5 Good Performance For Both Interpolation and Downsampling

One of the most natural requirements in interpolation and resizing is that when applied to an image with a constant pixel value, it should always create another image with the same value. Thus, a kernel's DC response, i.e., the function obtained when $s[n] \equiv 1$ should be also identical to one. This is possible only when we have an exact *partition of unity*:

$$\sum_{k=-\infty}^{\infty} \beta \cdot h(\beta \cdot [t - k]) = 1, \quad t \in [0, 1). \quad (32)$$

In the frequency domain this corresponds to

$$H(0) + 2 \sum_{n=1}^{\infty} H\left(\frac{n}{\beta}\right) \cos(2\pi nt) = 1, \quad t \in [0, 1). \quad (33)$$

Interpolation kernels commonly satisfy this property exactly by having $H(0) = 1$, and $H(n) = 0$, $n = 1, 2, \dots$. Others provide very good approximation with very small values of $|H(0) - 1|$ and $|H(n)|$, $n = 1, 2, \dots$.

The problem of using interpolation functions for downsampling is that while the condition above may be satisfied exactly for $\beta = 1$, it may not be a good approximation when $\beta < 1$.

For example, let us consider the kernel for linear interpolation (tent function)

$$h_l(t) = \begin{cases} 1 - |t|, & |t| < 1, \\ 0, & |t| \geq 1, \end{cases} \quad (34)$$

Its DC responses for $\beta = 1$ and $\beta = 0.7$ are shown in Figure 10. We can observe that this kernel satisfies the partition of unity condition when $\beta = 1$, but is clearly inadequate when $\beta = 0.7$. In fact, in the latter case, if the resampling offset is zero, then the sampled response will alternate between values that are about 10% too large, and 10% too small, i.e.,

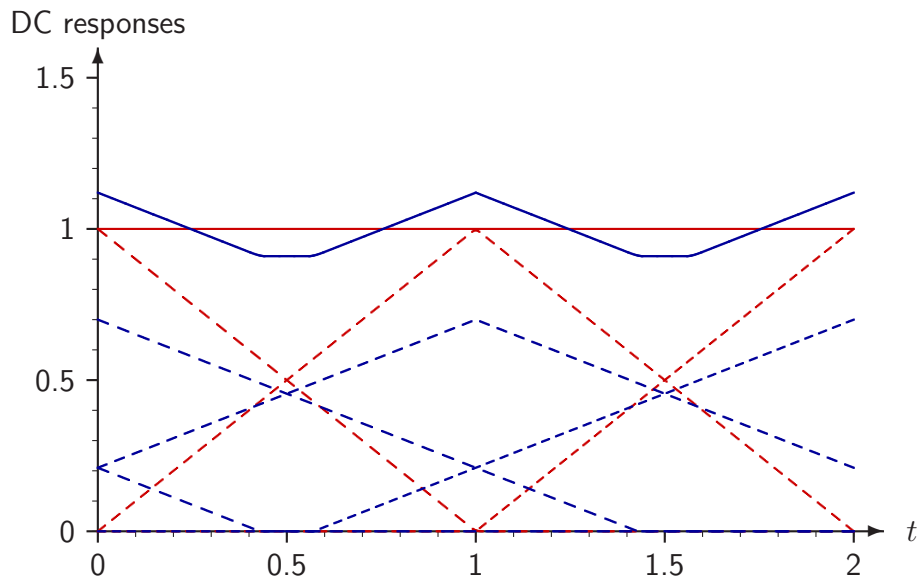


Figure 10: Sum of linear interpolation (tent function) kernels when $s[n] \equiv 1$. Dashed red lines correspond to shifted components and continuous red line to their sum when $\beta = 1$. The blue lines correspond to case $\beta = 0.7$.

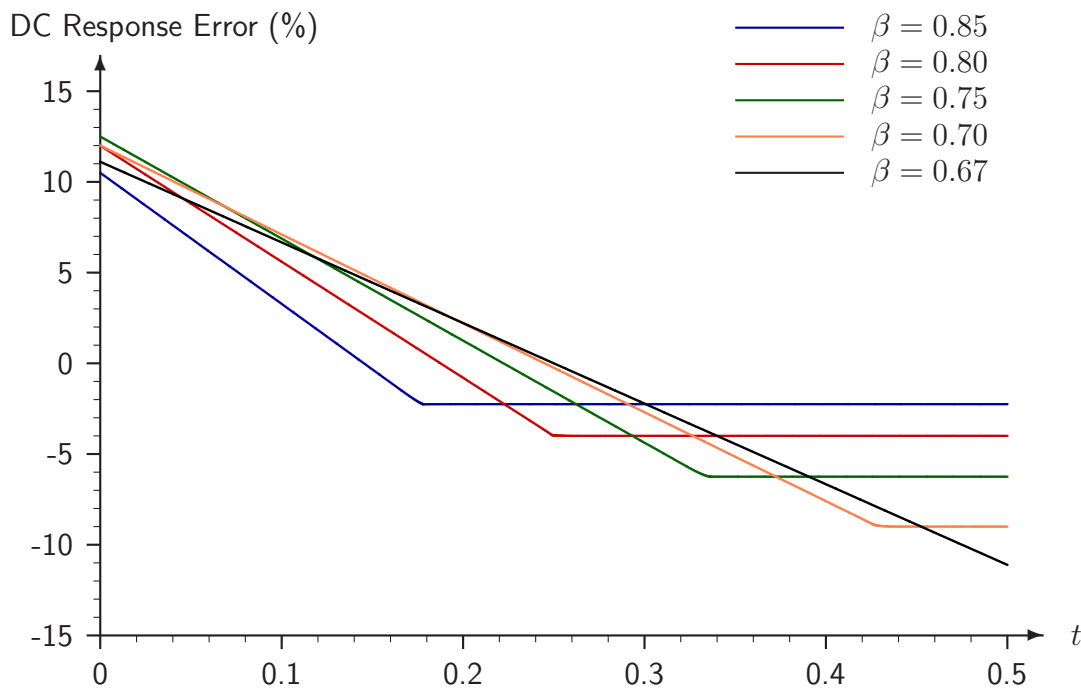


Figure 11: Error in the DC response for linear interpolation kernels.

Table 1: Parameters that approximate popular interpolation kernels.

Kernel	χ	η
Lanczos, $M = 2$	0.414	0.61
Lanczos, $M = 3$	0.284	0.64
Lanczos, $M = 4$	0.212	0.65
Lanczos, $M = 5$	0.170	0.65
Blackman-Harris, $N = 6$	0.411	0.23
Cubic B-Spline	0.310	0
Mitchell-Netravali, $B = C = 1/3$	0.550	0.32

an oscillation of about 20%! Figure 11 shows how the DC response error varies for other values of β .

Here we see one of the main advantages of kernel $h_{\chi,\eta}(t)$. With the proper choice of χ and η , the very fast decay guarantees that $|H_{\chi,\eta}(1/b)|$ is very small for $\beta < 1$, which means that it is also good as a downsampling filter. In the next section we present some example of this property and comparisons of the DC response errors (e.g., Figures 14 and 15).

6 Approximation of Other Kernels

Many of the features of the new kernels can be observed by analyzing versions that have parameters chosen to closely approximate kernels commonly used for interpolation. Table 1 shows some sets of parameters that can be used for these approximations, and Figures 12 and 12 show comparisons of the corresponding Fourier transforms. In Figure 12 we can observe that with $\chi = 0.248$ and $\eta = 0.48$ we have a response nearly identical to the Blackman-Harris ($N = 6$) kernel [1, 6]. Choosing $\chi = 0.163$ and $\eta = 1.2$ produces a response very similar to the Lanczos kernel ($M = 2$) [5, § 3] up to its first zero. After that, $H_{\chi,\eta}(f)$ produces a wider sidelobe with roughly the same height, but with nearly monotonic decay, instead of several sidelobes.

Figure 13 shows a comparison with another Lanczos kernel, with similar results. In part, these results are not very surprising, since the Blackman-Harris and Lanczos kernels are based on the $\text{sinc}(t)$ function. However, they show that we can get remarkable control of the properties of $H_{\chi,\eta}(f)$ by changing only its two parameters.

Furthermore, the comparison of $H_{\chi,\eta}(f)$ with the cubic b-spline kernel in Figure 13 shows that we can have very good approximations for other types of kernels too. One important difference, is that $H_{\chi,\eta}(f)$ has no sidelobes above -80 dB when $f > 1$, which means that it has better partition of unity when used for downsampling.

We also tested the Lanczos (LZ4), Blackman-Harris (BH6), and cubic b-spline (CBS)

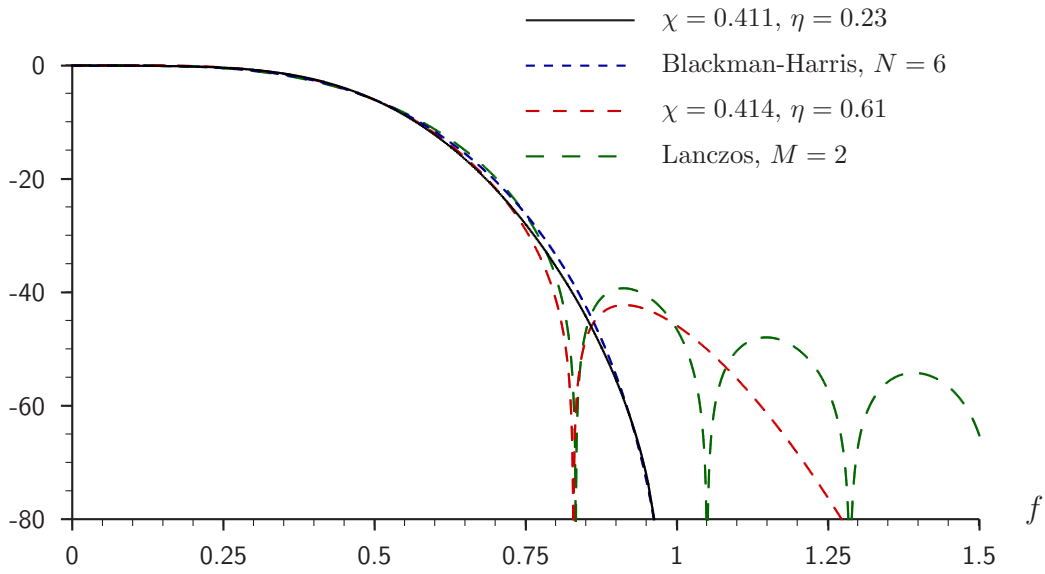


Figure 12: Fourier transforms of some commonly used kernels, and of their approximation with the proposed parameterized kernels. First set.

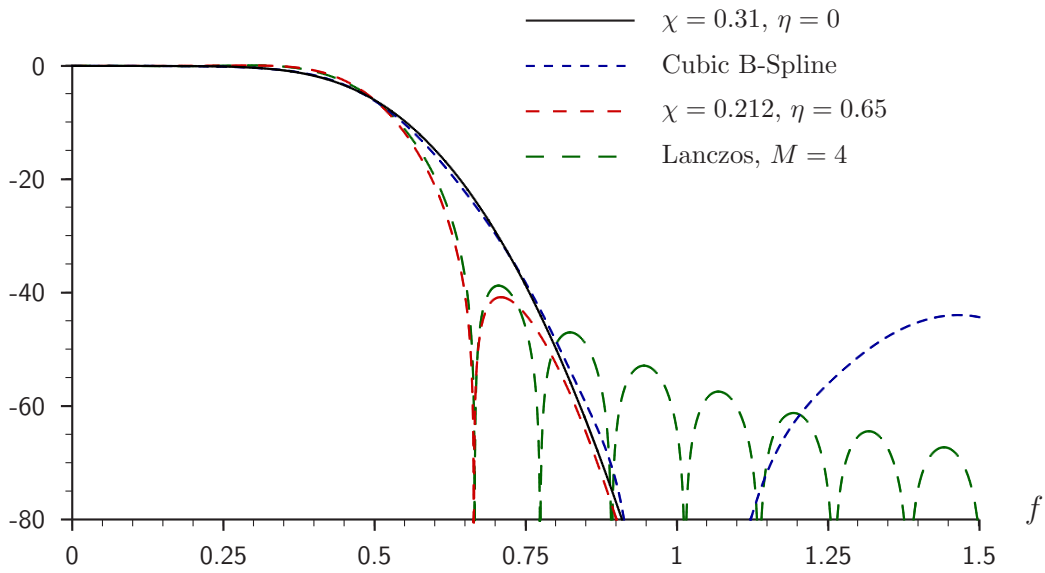


Figure 13: Fourier transforms of some commonly used kernels, and of their approximation with the proposed parameterized kernels. Second set.

kernels in the 2048×2560 image “Bike” (used in the JPEG2000 tests), chosen because it has many details and test patterns. First, we upsampled all images by factor 1.7. In all cases, the images are visually indistinguishable, so we measured the differences between images. The results, defined as PSNR in dB, are:

Kernel	LZ4	BH6	CBS
LZ4-Approx.	51.3	42.6	49.4
BH6-Approx.	43.4	58.3	48.4
CBS-Approx.	47.9	47.3	58.1

The values in the main diagonal show that the images obtained with the kernels and their approximations are indeed very close. The other values are also large, indicating that all those kernels produce good results, but the differences are also clear.

In the second experiment we downsampled the image by factor 0.6, and obtained similar results

Kernel	LZ4	BH6	CBS
LZ4-Approx.	51.4	38.9	45.6
BH6-Approx.	39.9	56.1	45.2
CBS-Approx.	45.2	44.0	57.0

As explained in Section 5.5, an advantage of the new kernels is that they present very fast decays on the frequency response, which can make them (depending on the parameters) better for downsizing because of the smaller error on the DC response. Figures 14 and 15 show comparisons of the DC response error for two kernel approximations. In Figure 14 we observe that while the cubic b-spline—which has ideal DC response when $\beta = 1$ —produces errors for other values of β . Its approximation, on the other hand, has not sidelobe ($\eta = 0$, cf. Figure 13), and consequently the very fast decay produces very small DC response errors. In fact, the error has a nearly constant it $-5 \cdot 10^{-6}$ for all values of $0 \leq t \leq 1$ and $0.5 \leq \beta \leq 1$. Figure 15 shows a similar comparison, with the Lanczos kernel. Note that in this case the DC response of the approximation is similarly nearly independent of t and β (in fact, $\beta = 1$ is commonly the worst case). However, there are error because η has a relatively large value.

7 Conclusions

We have shown that the proposed kernels for image interpolation and resizing can be easily designed, since their two parameters provide direct control over the most important features, which are the width of the transition band, and the sidelobe height. We also explain that

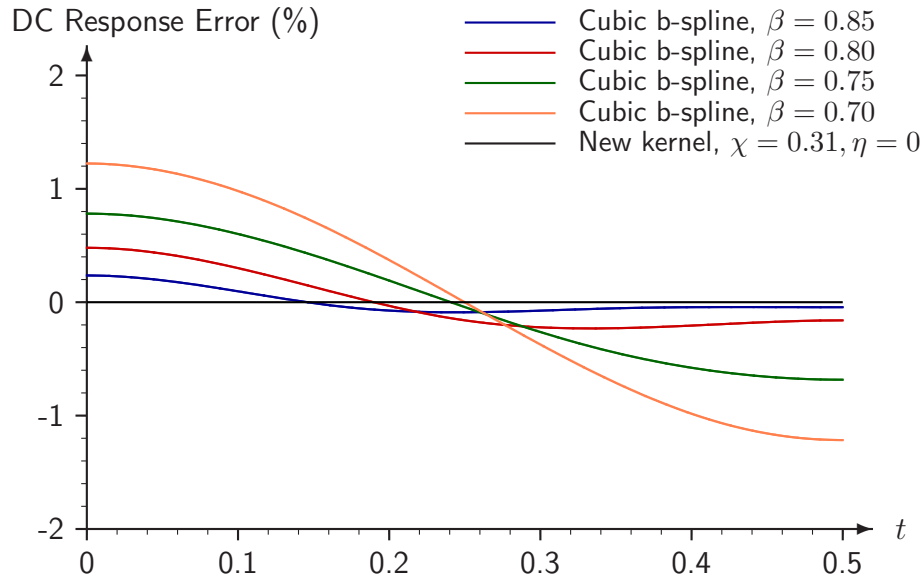


Figure 14: Comparison of DC response errors between the cubic b-spline kernel and its approximation. The error of the new kernel has a nearly constant value of $-5 \cdot 10^{-6}$ for all values of t and β in the graph.

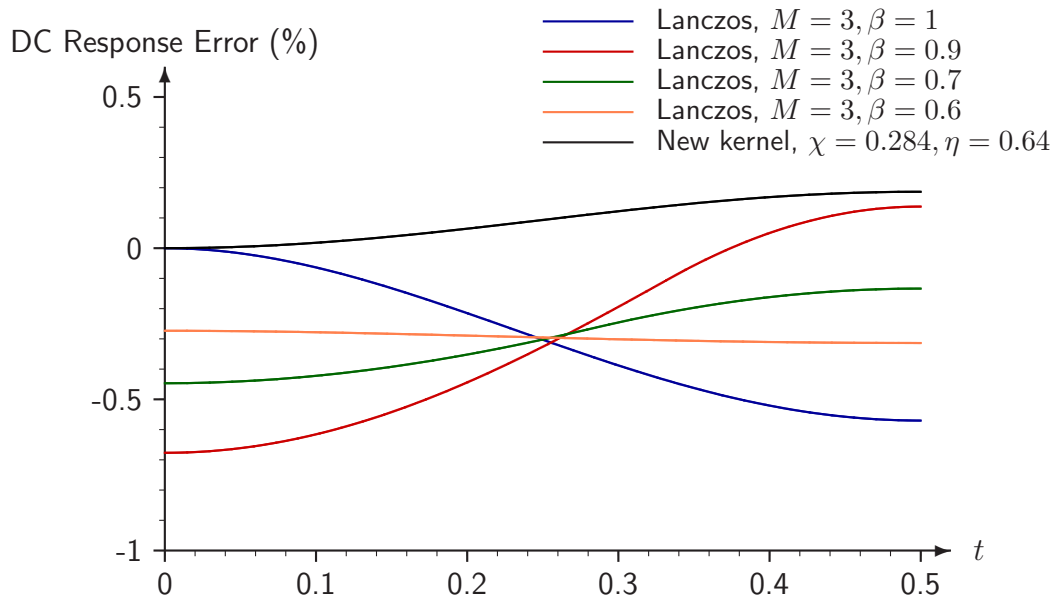


Figure 15: Comparison of DC response errors between the Lanczos kernel and its approximation.

the kernels naturally satisfy many desirable conditions. They yield exact interpolation, both the functions and their Fourier transforms have very fast decays, and thus the same kernels can produce good results for both interpolation and downsampling. We tested the flexibility of the design by presenting sets of parameters that produce kernels that are very good approximations of kernels that are well known for their properties and superior image quality. The differences between the original kernels and the approximations are evaluated by analyzing the frequency response, and also measuring the difference between images resized with those kernels. In conclusion, the new class of kernels provide a very convenient way to test different kernels in order to identify those that produce the best image quality.

References

- [1] F.J. Harris, “On the use of windows for harmonic analysis with the Discrete Fourier Transform,” *Proc. IEEE*, vol. 66, pp. 51–83, Jan. 1978.
- [2] D.P. Mitchell and A.N. Netravali, “Reconstruction filters in computer graphics,” *ACM Computer Graphics*, vol. 22, pp. 221–228, Aug. 1988.
- [3] A.V. Oppenheim and R.W. Schaffer, *Discrete-Time Signal Processing*, Prentice Hall, Englewood Cliffs, New Jersey, 1989.
- [4] R.C. Gonzalez and R.E. Woods, *Digital Image Processing*, Addison-Wesley Pub. Co., Reading, MA, 1992.
- [5] A.S. Glassner (ed.), *Graphics Gems*, Academic Press, San Diego, 1998.
- [6] T.M. Lehman, C. Gönner, and K. Spitzer, “Survey: interpolation methods in medical image processing,” *IEEE Trans. Medical Imaging*, vol. 18, pp. 1049–1075, Nov. 1999.
- [7] P. Thévenaz, T. Blu, and M. Unser, “Interpolation revisited,” *IEEE Trans. Medical Imaging*, vol. 19, pp. 739–758, July 2000.
- [8] E. Meijering, “A chronology of interpolation: from ancient astronomy to modern signal and image processing,” *Proc. IEEE*, vol. 90, March 2002.